

I- Initiation of Cardiac Electrical Activity

Automaticity & Rhythmicity of the Heart

- **Automaticity** → ability of the heart to initiate its own contraction independent of external stimuli
- **Rhythmicity** → heart can beat regularly
- Automaticity & rhythmicity are due to spontaneous & regular pacemaker AP
- **Pacemaker cells are present in SA node, AV node & Purkinje fibers:**
 - a. **SA node** → normal human pacemaker → fastest rate of AP (105/min)
 - b. If the SA node fails, → AV node (60/min) becomes the pacemaker
 - c. If the AV node fails, → Purkinje cells (40/min) become the pacemaker → idio-ventricular rhythm
 - d. SA node → 60-200 AP/min under various normal conditions
 - e. **"Vagal tone"**: normally, parasympathetic (vagal) effect on SA node is stronger than sympathetic → ---- SA node rate → normal resting HR = 72 beats/min

Pacemaker potential: 3 phases: phases 4, 0 & 3

Phase 4: Pre-potential or spontaneous gradual depolarization:

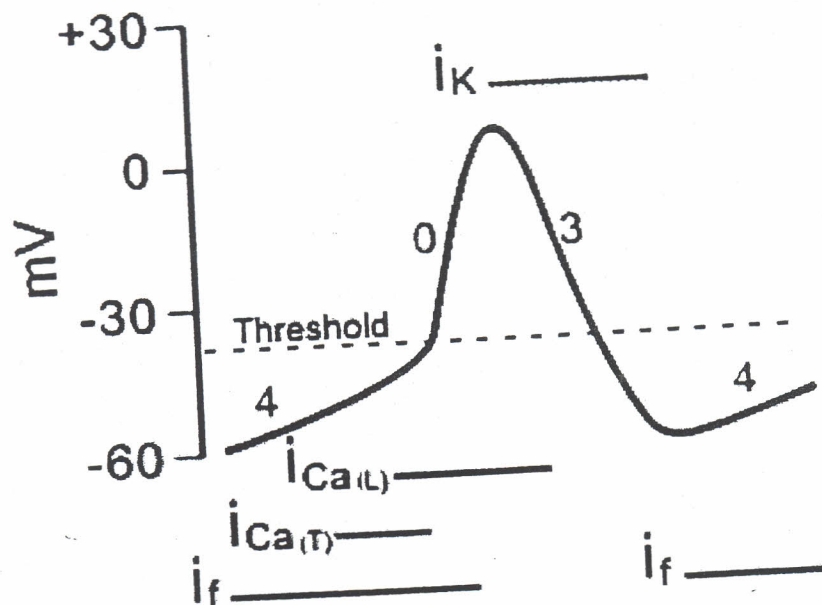
- a. At start, membrane potential is -60 mV → special slow Na^+ channels open → inward (depolarizing) **"funny" current (I_f)** → spontaneous depolarization
- b. At membrane potential -50 mV → transient **T-type Ca^{++} channels** open → inward Ca^{++} current (I_{CaT}) with electrochemical gradient → -40 mV.

Phase 0: At -40 mV (firing level) 2 events occur at same time:

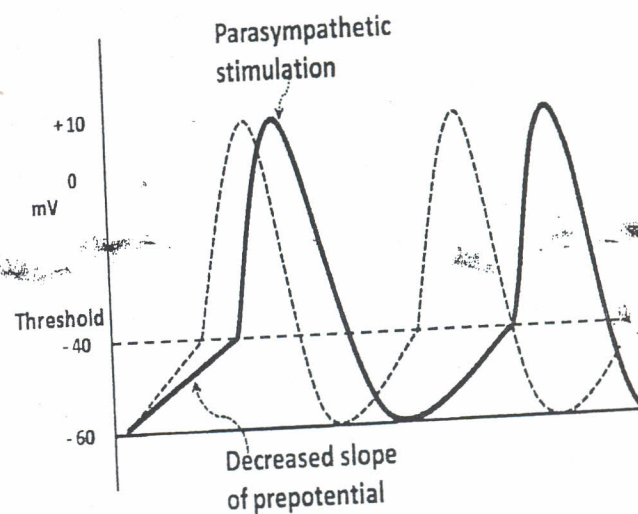
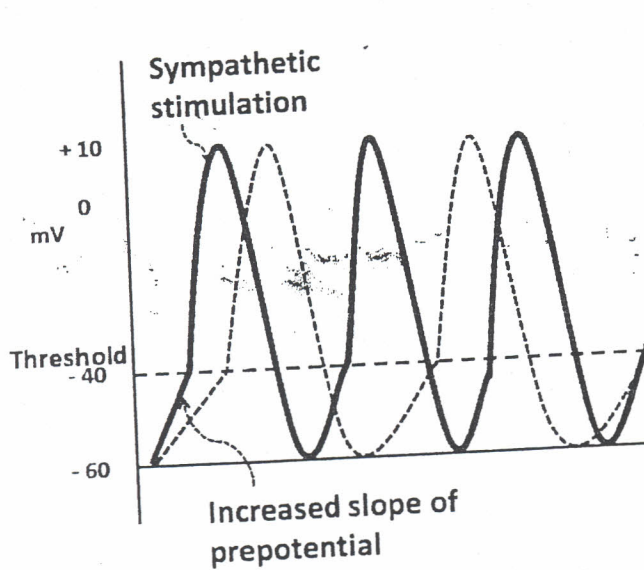
- a. Closure of "funny" current (I_f) & transient Ca^{++} current (I_{CaT}) channels
- b. Opening of long-lasting L-type Ca^{++} channels → more Ca^{++} entry (I_{CaL}) but not rapid → slow depolarization → "slow response AP"
- c. Depolarization → gradual opening of delayed rectifying K^+ channels

Phase 3: repolarization phase (2 events occur at same time):

- a. Opening of delayed rectifying K^+ channels → outward K^+ current (I_{K}) along its electrochemical gradient → repolarization
- b. Closure of LCa^{++} channels → stops inward depolarizing Ca^{++} currents (I_{CaL}).
- c. Repolarization continues until -60 mV → gradual inactivation of outward K^+ current (I_{K}), & activation of funny current (I_f) → spontaneous new phase 4



Figure(6): Pacemaker Action Potential with different ionic currents responsible for its phases.



Factors that affect the rate of discharge of SA node:

1- **Body Temperature:** $+++ t^{\circ}$ (fever) \rightarrow $+++$ HR (tachycardia). $+++1^{\circ} \rightarrow$ $+++10$ b/min

2- **Autonomic nerves activity:**

Sympathetic activity	Parasympathetic (vagal) activity
$+++$ discharge rate of SAN & HR (tachycardia) \rightarrow positive chronotropy <u>Mechanism:</u> **Sympathetic \rightarrow Norepinephrine $\rightarrow \beta_1$-adrenoreceptors \rightarrow $+++$ c-AMP \rightarrow $+++$ funny current \rightarrow $+++$ slope of phase 4 \rightarrow reach phase 0 more rapid	$---$ discharge rate of SAN & HR (bradycardia) \rightarrow negative chronotropy <u>Mechanism:</u> **Vagus \rightarrow Acetylcholine \rightarrow muscarinic receptors \rightarrow $----$ c-AMP \rightarrow $----$ funny current \rightarrow $----$ slope of phase 4 \rightarrow reach phase 0 in a longer time **Acetylcholine \rightarrow $+++$ K^+ channels (K_{Ach}) \rightarrow K^+ efflux \rightarrow opposes the funny current & $---$ the slope of phase 4 more & more

3- **Catecholamines:** Adrenal medulla \rightarrow epinephrine & norepinephrine \rightarrow $+++$ HR

4- **Extracellular K^+ level:**

- Hypokalemia** \rightarrow tachycardia
- Hyperkalemia** \rightarrow bradycardia

5- **Ca^{++} channel blockers** \rightarrow inactivation of L-type Ca^{++} channels \rightarrow bradycardia

II- Conduction of Action Potentials within the heart

Spread of AP between cardiac cells occurs through **gap junctions** \rightarrow direct electric conduction (Low electric resistance \rightarrow rapid transmission)

The velocity of conduction between cells depends on:

1- **Electrical resistance between cells:** The more the n= of gap junctions at intercalated discs \rightarrow the faster the conduction.

Hypoxia or $+++$ intracellular free $Ca^{++} \rightarrow$ $-----$ conduction through gap junctions

2- **Amplitude & speed of AP upstroke:**

Slow upstroke in SAN & AVN \rightarrow slow conduction

Initiation & propagation of cardiac impulse

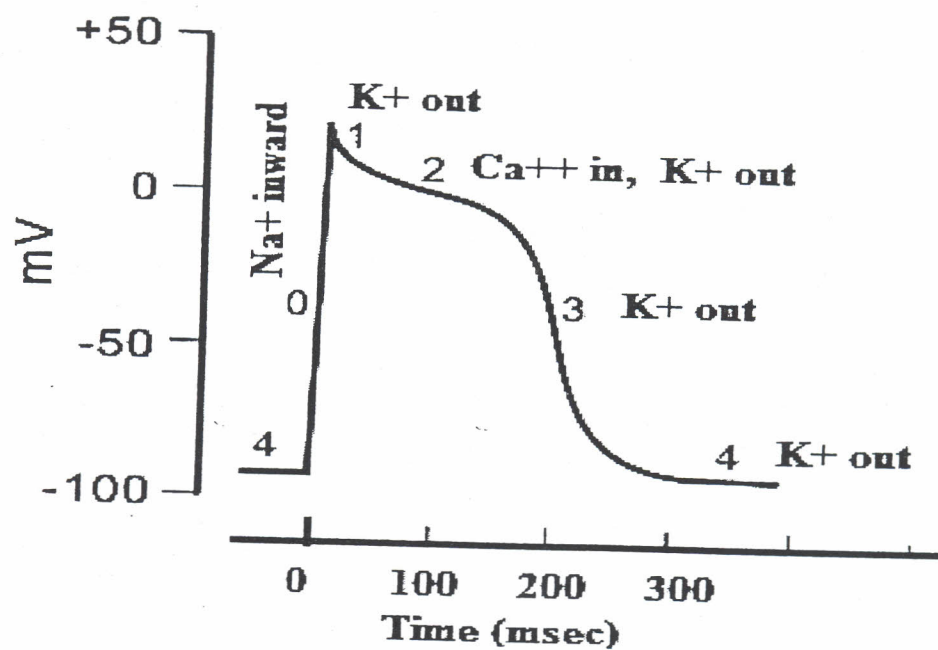
1. AP generated at SA node \rightarrow **atrial myocytes (0.5 m/sec).**

Internodal bundles transmit AP directly from SA node to AV node (1 m/sec).

2. AV node \rightarrow only pathway for transmission of AP from atria to ventricles

Conduction within the AV node is slow (0.05 m/sec) due to:

- Few gap junctions
- Slow upstroke of the AP



Importance of slow conduction within AV node:

- Delays arrival of AP from atria to ventricles for 0.1 sec → gives atria enough time to contract & fill the ventricles before they contract
 - Limits the rapid frequency of impulses from atria to ventricles in some diseases
3. AP from AV node → **bundle of His** → left & right **bundle branches** → **Purkinje fibers** (very rapid **4 m/sec** from subendocardium (in) to epicardium (out)) → AP reach all cells at same time → effective pumping
4. AP can spread from one **ventricular myocytes** to another at **0.5 m/sec**

5. Factors affecting the rate of conduction:

- +++Sympathetic → β_1 adrenergic receptors → +++ ionic conductance → faster AP upstroke → +++ rate of conduction
- +++Parasympathetic → muscarinic receptors → --- ionic conductance → slower AP upstroke → --- rate of conduction
- Digitalis → +++ parasympathetic activity → ---- conduction velocity

III- Cardiac Myocyte (Non-pacemaker) Action potential

Rapid depolarization from RMP (-90 mV) to firing level (-65 mV) by cell-to-cell conduction of depolarizing potential; Cardiac AP is then generated:

Phase 4 = RMP

- continues till cardiac cells become depolarized
- K^+ slowly moves out (I_{K1}) through **inward rectifying potassium channels**.

Phase 0 = depolarization

- rapid upstroke of AP from resting value to +20 mV
- influx of Na^+ through **fast Na^+ -channels** → inward depolarizing current (I_{Na})
- --- K^+ conductance due to inactivation of inward rectifying K^+ channels
- Fast Na channels are inactivated (fast upstroke) → "**fast response AP**".

Phase 1 = rapid small initial repolarization

- inactivation of fast Na^+ channels
- efflux of K^+ through **transient outward K^+ channels** → transient outward repolarizing current (I_{to})

Phase 2 = plateau

Membrane repolarization slows down → sustained around zero mV for 200 msec due to a balance between:

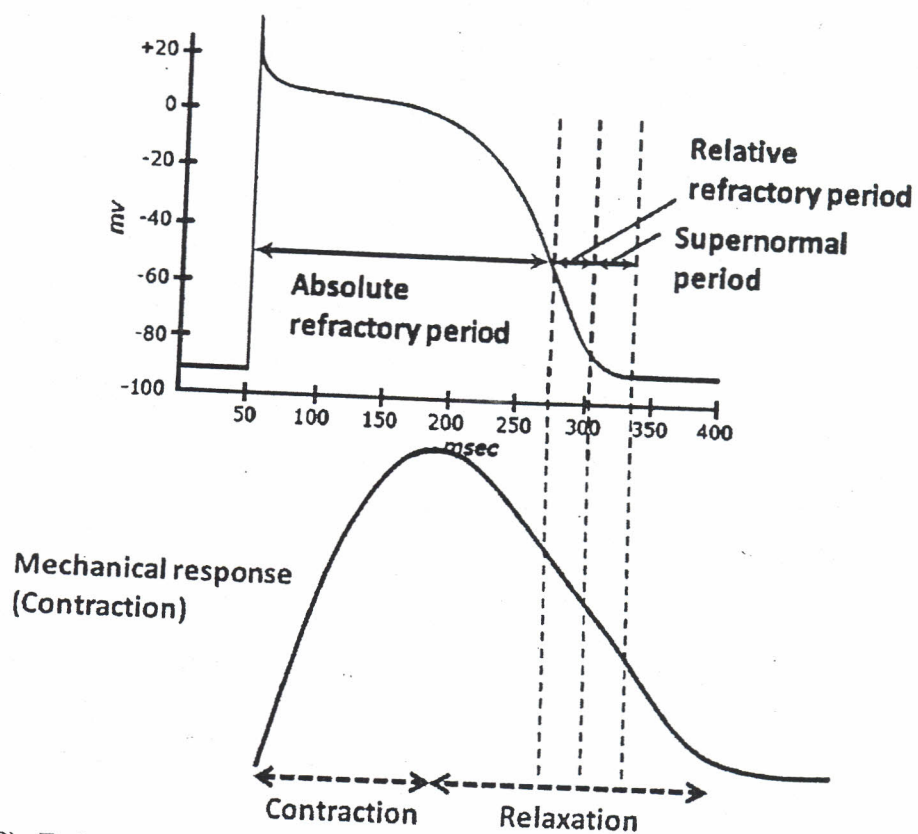


Figure (9): Relation between ventricular action potential and mechanical response (contraction).

- Inward positive current:

- **Inward Ca^{++} current, through **long lasting Ca^{++} channels (I_{CaL})**.

- Channels start to open at -40 mV in phase 0 → fully active in phase 2
 - Remain open for long time → spontaneous inactivation = time-dependent

- ** Na^{+} - Ca^{++} exchanger activity near the end of plateau (due to Ca^{++}) → 1Ca^{++} out & 3Na^{+} in (net → 1 +ve ion influx) → prolongs the plateau

- Outward positive K^{+} current through **delayed rectifier K^{+} channels (I_{K})**

Phase 3 = rapid repolarization

- long lasting Ca^{++} channels closed
- **delayed rectifier K^{+} channels** → maximally active → outward K^{+} current (I_{K}) → repolarization (-80 to -85 mV) → gradual closure of delayed rectifier K^{+} channels
- **inward rectifying K^{+} channels** → gradually open → outward repolarizing current (I_{K1}) → complete repolarization to RMP (-90 mV)

Relationship between AP & contraction in cardiac myocyte

- Contraction → starts just after beginning of AP → reaches maximum at end of plateau (phase 2).
- Repolarization (phase 3) → coincides with 1st half of relaxation.

Excitability changes during action potential

1- Absolute refractory period ARP:

- Phases 0, 1, 2 & part of 3 → zero excitability (all Na channels are opened in phase 0 & inactivation gates are closed in phases 1 & 2)
- ARP → occupies contraction & early relaxation → prevent tetanic contractions

2- Relative refractory period RRP:

Phase 3 of AP → supra-threshold stimulus can elicit a new AP

3- Supernormal period (vulnerable period):

Late part of phase 3 → can respond to a weaker stimulus → arrhythmias

Mechanical Properties of Cardiac Muscle

Excitation contraction coupling

- 1- Membrane depolarization → open L-type Ca^{++} channels → Ca^{++} enter → Ca^{++} below sarcolemma → open "ryanodine- Ca^{++} release channel" in terminal cisterns of SR → Ca^{++} release from SR ("Calcium-induced Calcium release").

- 2- Ca^{++} binds to Troponin-C \rightarrow contraction as described for skeletal muscle
- 3- Ca^{++} release decreases when AP ends.

4- Relaxation: Ca^{++} is removed from the cytoplasm by:

- a. Ca^{++} pump into SR (sarco-endoplasmic reticulum calcium ATPase, "SERCA")
- b. Ca^{++} is transported into ECF by:
 - $\text{Na}^{+}\text{-Ca}^{++}$ exchanger
 - Ca^{++} pump

$\text{Ca}^{++} \rightarrow$ determines the force of contraction (**contractility** or **inotropic state**).

Ca^{++} release during rest is not maximal. More Ca^{++} release \rightarrow +++contractility/+++force (+ve inotropic). Less Ca^{++} release \rightarrow ----contractility/----force (-ve inotropic)

Regulation of Contractility (inotropic state) of cardiac myocytes

Positive inotropic mechanisms	Negative Inotropic Mechanisms
1- +++ sympathetic or catecholamines \rightarrow +++ β -adrenergic receptors \rightarrow +++ c-AMP \rightarrow activates Protein Kinase A (PKA) \rightarrow +++ Ca^{++} in cells: <ol style="list-style-type: none"> a. PKA phosphorylates L-Ca^{++} channel \rightarrow open for longer time \rightarrow enter more Ca^{++} b. PKA phosphorylates certain sites on SR \rightarrow more Ca^{++} release 	1- Ischemia to cardiac muscle (---blood supply) \rightarrow hypoxia \rightarrow ----ATP energy for contraction
2- Glucagon \rightarrow +++ c-AMP in myocytes	2- +++ parasympathetic (vagus) \rightarrow acetylcholine \rightarrow +++ muscarinic M2 receptors \rightarrow ---c-AMP
3- +++ECF- Ca^{++} concentration \rightarrow +++ Ca^{++} entry	3- Adenosine \rightarrow ----c-AMP production
4- Drugs: <ol style="list-style-type: none"> a. Digitalis \rightarrow inhibits $\text{Na}^{+}\text{-K}^{+}$ ATPase \rightarrow +++ Na^{+} in \rightarrow +++ $\text{Na}^{+}\text{-Ca}^{++}$ exchanger \rightarrow moves Na^{+} out & Ca^{++} in \rightarrow +++ Ca^{++} in b. Xanthines (caffeine) \rightarrow ---- c-AMP breakdown \rightarrow +++ c-AMP in myocytes 	4- Drugs: <ol style="list-style-type: none"> a. Ca^{++} channel blockers (dihydro-pyridine) \rightarrow inhibit L-Ca^{++} channels \rightarrow ----Ca^{++} entry b. Anesthetic drugs.

Regulation of Myocyte Relaxation (lusitropy)

- 1- +++ β -adrenergic receptors \rightarrow +++ c-AMP & PKA \rightarrow accelerate relaxation by:
 - a. Activation of SERCA pump \rightarrow rapid removal of Ca^{++} by SR \rightarrow rapid relaxation
 - b. Decreased binding of Troponin to Ca^{++} .
- 2- Myocardial ischemia inhibits relaxation (+++ Ca^{++} permeability \rightarrow +++++ Ca^{++} in \rightarrow inhibits relaxation (weak contraction & poor relaxation)

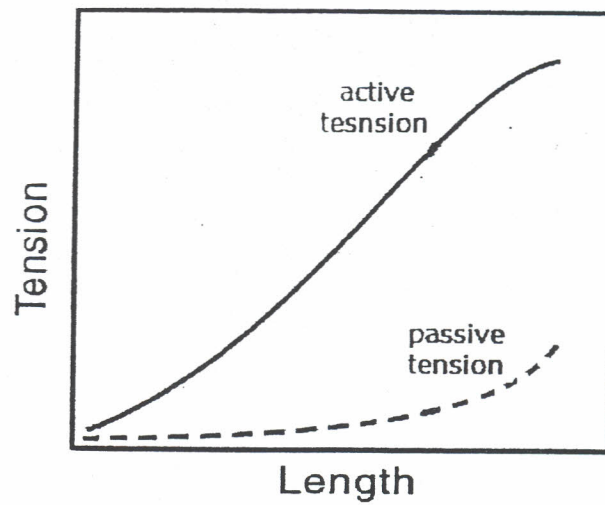


Figure (39): Passive and active length-tension relationships.

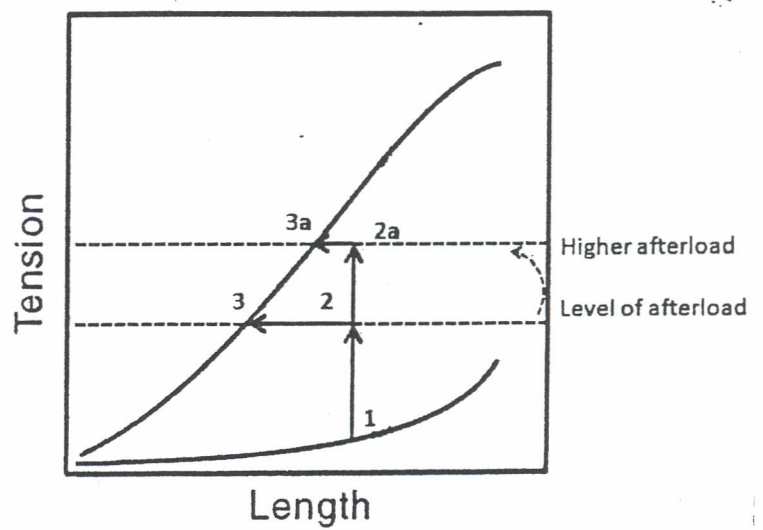


Figure (41): Effect of increasing afterload on cardiac muscle shortening.

Isometric and Isotonic contraction of isolated cardiac muscle

Isometric Contraction	Isotonic contraction
<ul style="list-style-type: none"> Isolated cardiac muscle → fixed to holder & attach a heavy load to its lower end. Load stretches the muscle to certain degree; Stimulate the muscle → contracts → maximum tension → but not able to shorten (heavy load) Sarcomeres are shortened → stretch of elastic elements +++ the tension in muscle to maximum while its length remains constant 	<ul style="list-style-type: none"> Same muscle but using small load Muscle is stretched to same degree; Stimulate the muscle → contraction starts isometric → +++ muscle tension till = load Muscle shortens & lift the load Tension remains constant

What is meant by “preload” and “afterload”?

Preload → degree of stretching of cardiac muscle before it contracts

Afterload → load against which the muscle contracts: load lifted by the muscle;

- isotonic contraction → if the muscle succeeds to lift the load;
- isometric contraction → if the muscle could not lift the load

Length-Tension Relationship in Cardiac Muscle

a. Passive length-tension relationship:

Passive stretch of cardiac muscle → +++ tension within the muscle

b. Active length-tension relationship: **Frank-Starling Law:**

Within limits, tension developed during isometric contraction is directly proportional to the degree of stretching of the muscle (i.e. preload).

Performance of Cardiac Muscle

Indicators of performance:

- 1- Degree of shortening: (length-tension diagram)
- 2- Velocity of shortening: (load-velocity relationship)

1- Effect of changing afterload on cardiac muscle performance

a- Effect of changes in afterload on muscle shortening:

- +++ afterload → ---- degree of shortening (inverse relationship)
- The muscle starts isometric contraction at same preload (1).
- +++ tension to be equal to the new higher afterload (2a).
- Contraction becomes isotonic & muscle shortens (3a).
- Degree of shortening is smaller (distance between 2a & 3a).

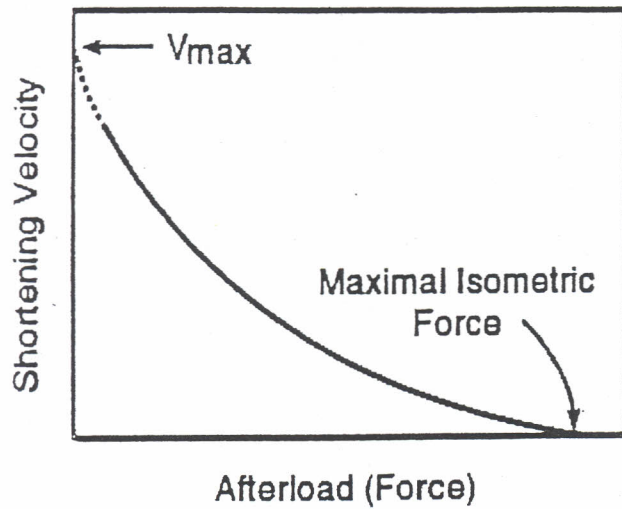


Figure (42): Effect of increasing afterload on velocity of shortening of cardiac muscle.

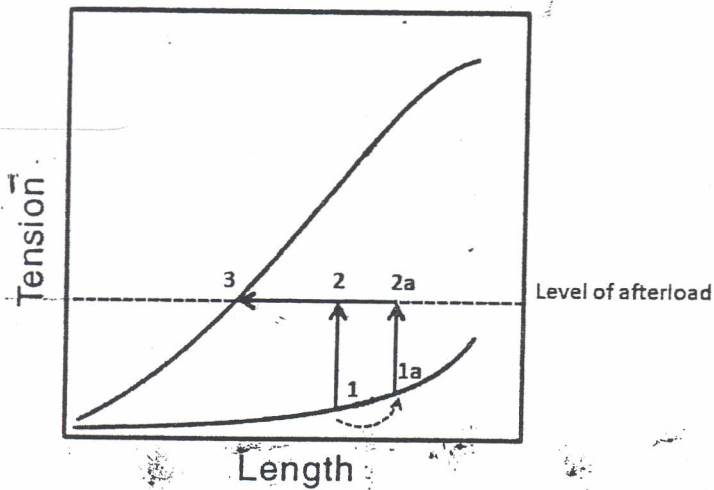


Figure (43): Effect of increasing preload on cardiac muscle shortening.

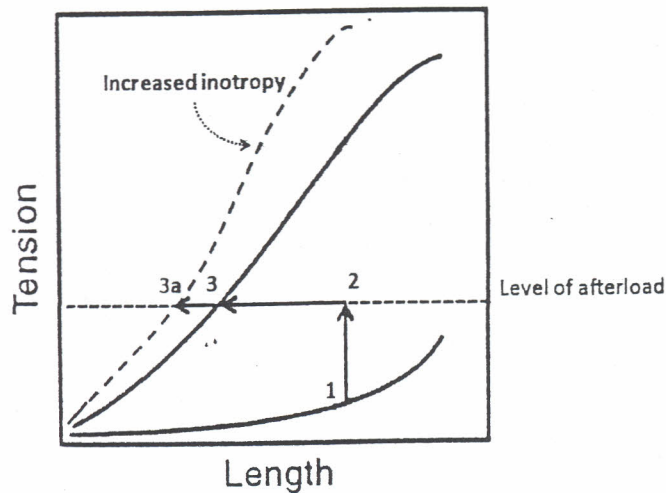


Figure (45): Effect of increased inotropy on degree of shortening of cardiac muscle.

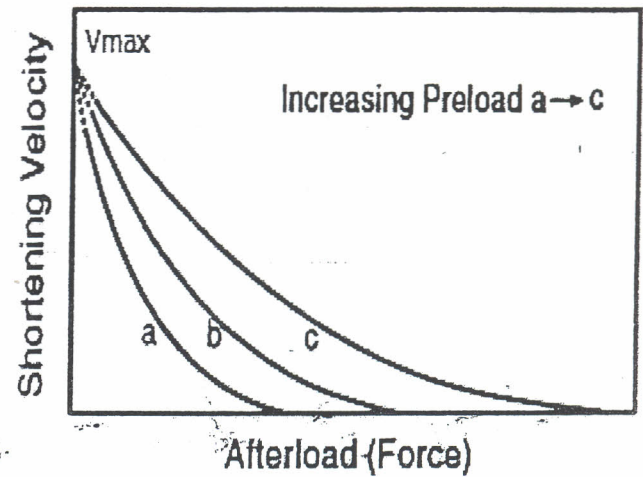


Figure (44): Effect of increasing preload on velocity of shortening of cardiac muscle.

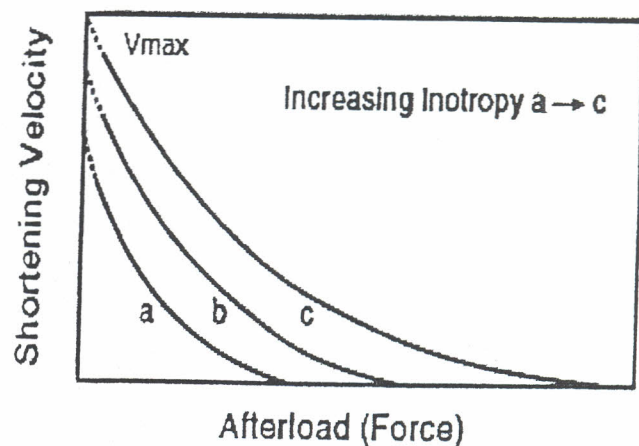


Figure (46): Effect of increased inotropy on the velocity of shortening of cardiac muscle.

b- Effect of changes in afterload on velocity of shortening:

- +++ afterload → ---- velocity of shortening (inverse relationship)
- Zero Velocity of shortening → when load \geq maximum isometric tension
- Maximal velocity of shortening (V_{\max}) → when load = zero (extrapolation) (muscle can't contract against zero load))

2- Effect of changing preload on cardiac muscle performance

a- Effect of changes in preload on muscle shortening:

- +++ preload → +++ degree of shortening (directly proportional)
- +++ preload → stretch the muscle to higher length (1a)
- Muscle contracts isometrically to the same level of afterload (2a)
- Then muscle contracts isotonicly (3)
- Degree of shortening is greater (distance between 2a & 3)

b- Effect of changes in preload on velocity of shortening:

- +++ preload → +++ velocity of shortening (V_{\max} is not changed)
- +++ preload shifts load-velocity curve up & right

3. Effect of changing inotropic state on cardiac muscle performance

a- Effect of changes in inotropic state on muscle shortening:

- +ve inotropics → shifts length-tension relationship up & left (+++ shortening)
- -ve inotropics → shifts length-tension relationship down & right (--- shortening)

b- Effect of changes in inotropic state on velocity of shortening:

- +ve inotropics → shifts load-velocity curve up & right (faster contraction)
- +++ V_{\max} (changed only by +ve inotropics); thus V_{\max} → index of contractility
- -ve inotropics → the opposite occurs

1. Effect of changing frequency of stimulation on force of contractions

+++ frequency → gradual +++ in force of contractions (inotropy) → "staircase phenomenon" / "treppe" : rapid repetition of contractions → no enough time for complete removal of released Ca^{++} → +++ Ca^{++} in cytoplasm & +++ force of contraction

Cardiac Cycle (systole & diastole)

Ventricular systole: 2,3,4

Ventricular diastole: 5,6,7,8,1

Early diastole: 5,6

Mid- diastole: 7,8

Late diastole: 1

Phase	1: Atrial Systole	2: Isovolumetric Contraction	3: Rapid Ejection	4: Reduced Ejection
Time	(0.1 sec)	(0.05 sec)	(0.15 sec)	(0.1 sec)
ECG	Initiated by P wave	Starts by QRS		start of "T" wave
Atrial pressure	+++ → ("a" wave) • Limited backflow of blood into vena cavae (contraction of atria → narrow orifices of veins) • Atrial contraction → 30% of ventricular filling during rest; (shares more during exercise)	Small +++ → ("c" wave) (bulging of cusps inside the atria }	sharp small --- due to pulling of cusps downward	+++ due to accumulation of venous blood in atria → "v" wave
Ventricular pressure	+++ (left → 9mmHg; right → 4mmHg)	+++ (Left → 80mmHg; right → 10mmHg)	+++ (left → 120mmHg; right → 25mmHg)	---- & finally becomes lower than arterial pressure;
Ventricular volume	+++ → end-diastolic volume "EDV" (130 ml).	Constant	---- rapidly due to blood ejection	---- slowly End-systolic volume "ESV" = (60 ml) Stroke volume "SV" = (70 ml) $EDV - ESV = SV$ (130ml - 60ml)
AV valves	opened	Closed (ventricular pressure > atrial pressure)	Closed due to high ventricular pressure	Closed (ventricular pressure > atrial pressure)
Semilunar valves	Closed (as Ventricular pressure < arterial pressure)	Closed (ventricular pressure < arterial pressure)	Opened → blood ejection	
Heart sounds	4 th HS ... "S ₄ "	1 st HS... "S ₁ " (Closure of AV valves)		

aortic & pulmonary pressures	Gradual decrease (blood leave them peripherally)	---- → 80mmHg in aorta & 10mmHg in pulmonary	+++ → aorta:120mmHg; pulmonary: 25mmHg	---- but > than ventricular pressure Ejection continues due to momentum of ejected blood
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Phase	5: Protodiastolic	6: Isovolumetric Relaxation	7: Rapid Filling	8: Reduced Filling
Time	(0.04 sec)	0.06 sec	0.1 sec	0.2 sec
Atrial pressure	Period between the end of ventricular contraction & closure of semilunar valves Blood tends to flow back into the ventricles but prevented by closure of semilunar valves	+++Atrial pressure due to +++ venous blood ("v" wave)	---Atrial pressure rapidly due to rapid flow of blood out of them	Small decrease
Ventricular pressure		rapid drop in ventricular pressure to below arterial pressure	--- Ventricular pressure in spite of filling; because they relax during early filling.	+++Ventricular pressure as they fill with blood.
Ventricular volume		Constant (A-V & semilunar valves are closed)	+++ rapidly due to rapid filling by pressure gradient → passive filling (70% during rest)	+++ slowly due to slower filling
AV valves		Closed Ventricular pressure > atrial pressure	opened ventricular pressure < atrial pressure	
Semilunar valves		closed	closed	Closed
Heart sounds		Sudden closure of semilunar valves → "2 nd HSS ₂ ".	"3 rd HS S ₃ ".	
aortic & pulmonary pressures		---- Arterial pressure gradually due to flow of blood to peripheral vessels	----Arterial pressure as blood flows to the periphery	Arterial pressure continues to decrease

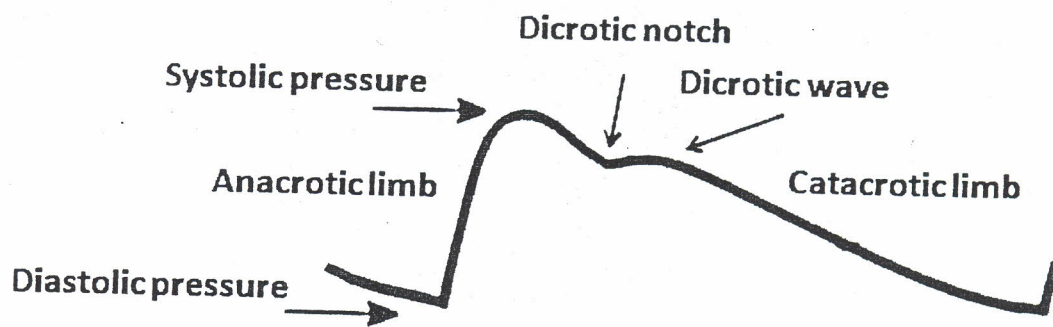


Figure (50): Aortic pressure curve.

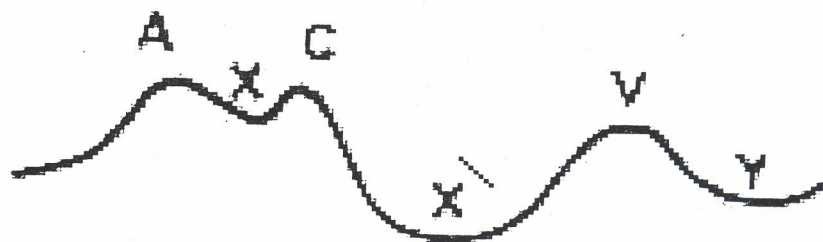
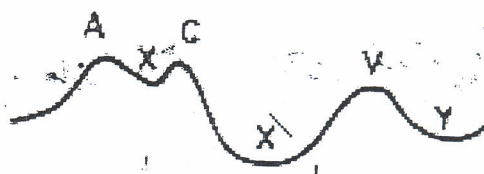


Figure (51): Jugular venous pulse curve.



CAROTID PULSE



JUGULAR PULSE

Aortic Pressure Curve = aortic pressure changes during cardiac cycle

Ascending limb "anacrotic limb":

It coincides with maximal ejection phase.

+++Aortic pressure to maximum (120mmHg) → **systolic arterial blood pressure**

Descending limb "catacrotic limb":

It coincides with the rest of cardiac cycle

----Aortic pressure to minimum (80mmHg) → **diastolic arterial blood pressure**

The following is observed on the catacrotic limb:

- Dicrotic notch, due to sudden closure of aortic valve at the end of systole.
- Dicrotic wave, due to elastic recoil of aorta → +++ aortic pressure

Right Atrial Pressure Curve and the "Jugular Venous Pulse JVP"

- No valves exist between the right atrium & superior & inferior vena cava.
 - Pressure changes occurring in right atrium during cardiac cycle are transmitted to these veins & Jugular vein:
1. "a" positive wave: → atrial contraction
 2. "x" negative wave: → atrial relaxation
 3. "c" positive wave: → bulging of tricuspid valve inside the right atrium during isovolumetric contraction phase
 4. "x" negative wave: → downward pull of A-V ring by ventricular contraction during rapid ejection phase
 5. "v" positive wave: → accumulation of venous return in right atrium while the tricuspid valve is closed
 6. "y" negative wave: is due to flow of blood out of the right atrium after opening of tricuspid valve during ventricular filling phase

Relationship between JVP & carotid pulse:

- "x" negative wave occurs with carotid pulse → jugular veins collapse normally with carotid pulsation
- "v" wave occurs with descending limb of carotid pulse (with collapsing carotid pulse)

Ventricular pressure-volume relationship: Pressure-Volume Loop:

The relationship between degree of stretch of cardiac muscle & developed tension in isolated cardiac muscle → can be applied to the ventricle with these modifications:

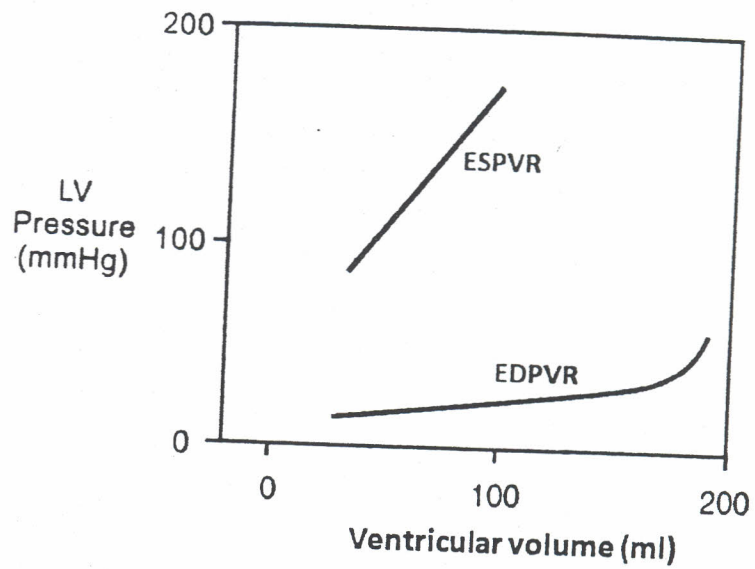


Figure (53): End-diastolic and end-systolic pressure-volume relationship.

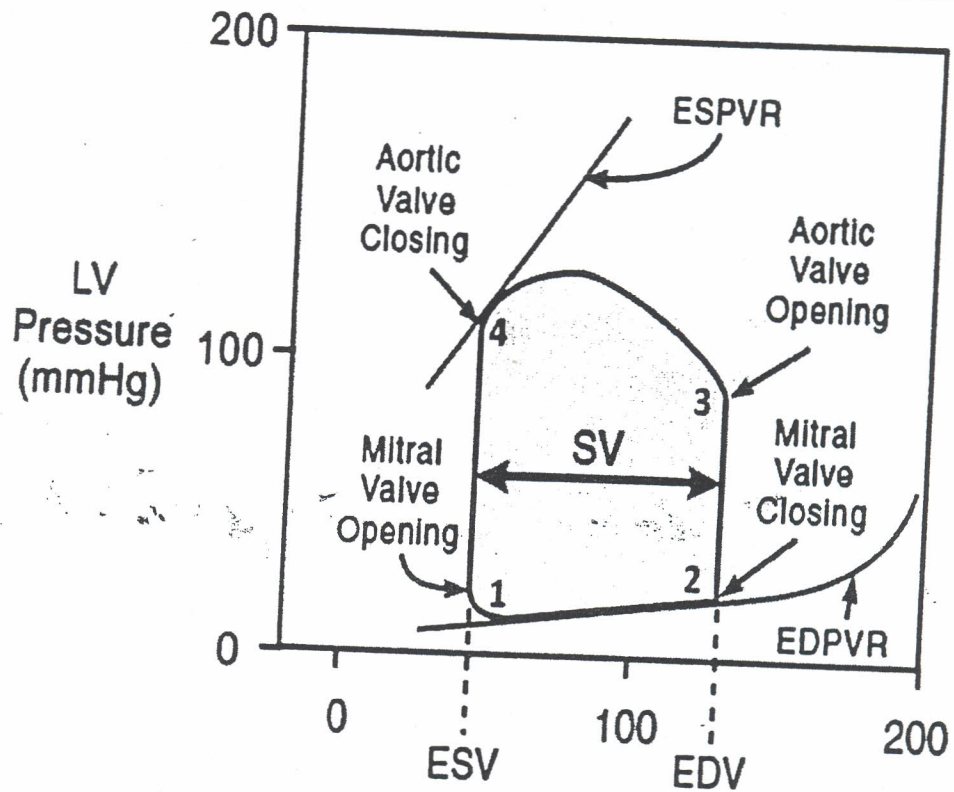


Figure (54): Left Ventricular Pressure-Volume loop.

length-tension relationship for isolated cardiac muscle	Pressure-Volume loop of whole heart
Degree of stretch	volume of ventricle at end of diastole (EDV)
tension	intraventricular pressure
passive length-tension relationship	"end-diastolic pressure-volume relationship EDPVR"
Tension developed during isometric contraction	maximal pressure developed in ventricle during contraction while the aorta is clamped ("end-systolic pressure" ESP)= isometric contraction
active length-tension relationship	"end-systolic pressure-volume relationship ESPVR"

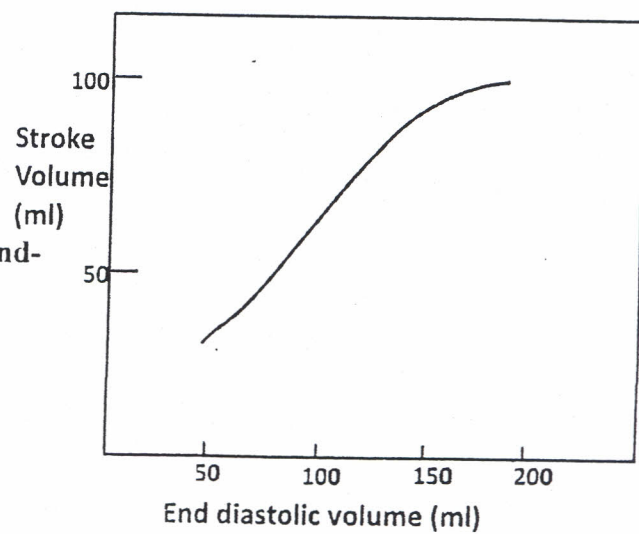
NB: Slope of the ESPVR depends on inotropic state of ventricular muscle.

- +ve inotropics → +++ the slope of ESPVR (shifts the ESPVR up & left)
- ve inotropics have an opposite effect

Pressure-volume loop during a complete cardiac cycle: changes in ventricular pressure in relation to changes in ventricular volume

- At beginning of diastole, ventricular volume = "end-systolic volume ESV" (1)
- Ventricle fills with blood → +++pressure till the "EDV" (2). Line "1-2" → ventricular filling phase
- Ventricle contracts isometrically (2) → mitral valve closes → 1st HS & +++ ventricular pressure (3). Line "2-3" → isometric contraction phase
- At "3", intraventricular pressure > aortic pressure → aortic valve opens
- Ejection of blood starts → ---- ventricular volume but +++ ventricular pressure to maximum then ---- again → end of systole ("4"). Line "3-4" → ejection phase
- At end of systole → Intraventricular pressure = ESP ("4" on ESPVR)
→ Ventricular volume = ESV
- Ventricular relaxation starts → ----Ventricular pressure < aortic pressure → aortic valve closes → 2nd HS (at "4").
- Isometric relaxation continues till intraventricular pressure < atrial pressure → mitral valve open ("1"). Line "4-1" → isometric relaxation phase
- Now, the ventricle starts to fill and a new cycle starts.
- Width of the pressure volume loop → stroke volume (SV)

Figure (56): Direct relationship between preload (end-diastolic volume) and Stroke volume.



Cardiac Output

Cardiac output (CO): volume of blood pumped by each ventricle/minute (5 L/min)

Cardiac Index (CI): $CI = CO \text{ (L/min)} \div \text{body surface area (m}^2\text{)} = 3.2 \text{ L/min/m}^2$

Cardiac output increases in	Cardiac output decreases in
1- Physical exercise (up to 700%). 2- Anxiety and excitement (up to 100%). 3- After meals (30%). 4- High environmental temperature. 5- Pregnancy.	1- Standing from supine position (30%) 2- Rapid cardiac arrhythmias and many other heart diseases.

Determinants of Cardiac output: Heart rate & Stroke volume

$CO = \text{stroke volume (SV)} \times \text{heart rate (HR)}$

Stroke volume = volume of blood ejected by each ventricle each heart beat

Heart rate = number of beats per minute

Control of Cardiac Output

I- Effect of changes in heart rate on cardiac output

- Changes in HR are quantitatively more important than changes in SV.
- +++HR during exercise 100-200% while +++ SV by 50% in untrained person
- HR is controlled mainly by autonomic nerves & some other factors
- +++ HR alone from 70-140 beat/min \rightarrow no change in CO (because of ----- ventricular filling \rightarrow -----SV \rightarrow thus no change in CO)
- +++ HR alone above 150/min \rightarrow ---- CO (marked ---- in SV can't be compensated by the +++ in HR)
- ---- HR alone below 60/min \rightarrow ---- CO (marked ---- in HR can't be compensated by the +++ in SV)
- During muscular exercise, +++ HR (doubled) \rightarrow +++ CO (more than double) because of the associated +++ in SV (+++sympathetic)

II- Regulation of Stroke Volume

1- Effect of changes in preload on stroke volume

- Preload = degree of stretch of cardiac myocytes before they start to contract (at end of diastole); measured by the sarcomere length
- EDV \rightarrow index of sarcomere length (index of preload)
- EDV depends on venous return (VR); +++ VR \rightarrow +++ EDV & the preload

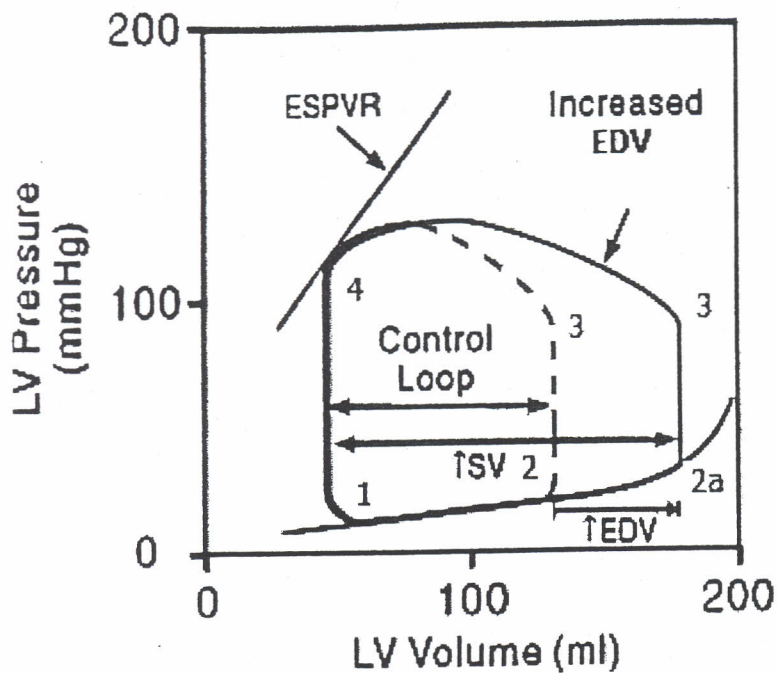


Figure (57): Effect of increasing preload (EDV) on pressure-volume loop, showing increased stroke volume (dashed-line loop is control loop before increasing EDV)

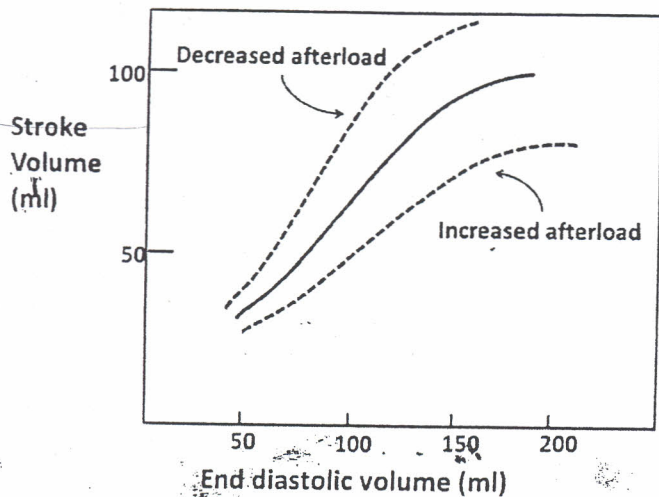


Figure (58): Effect of changing afterload on stroke volume.

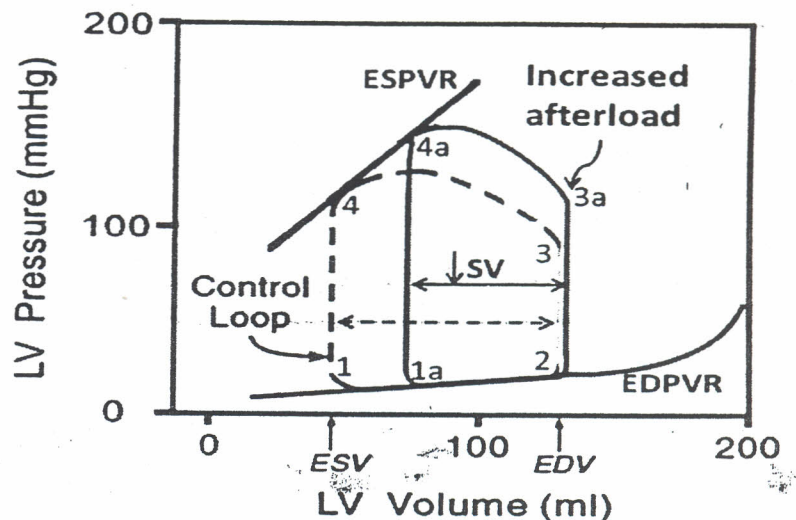


Figure (56a): Effect of sudden increase in afterload on pressure-volume loop, showing decreased stroke volume.

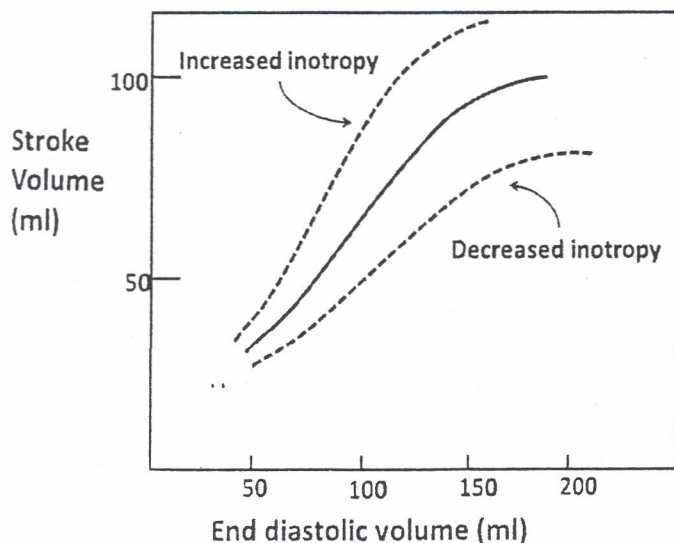


Figure (60): Effect of changing inotropy on stroke volume.

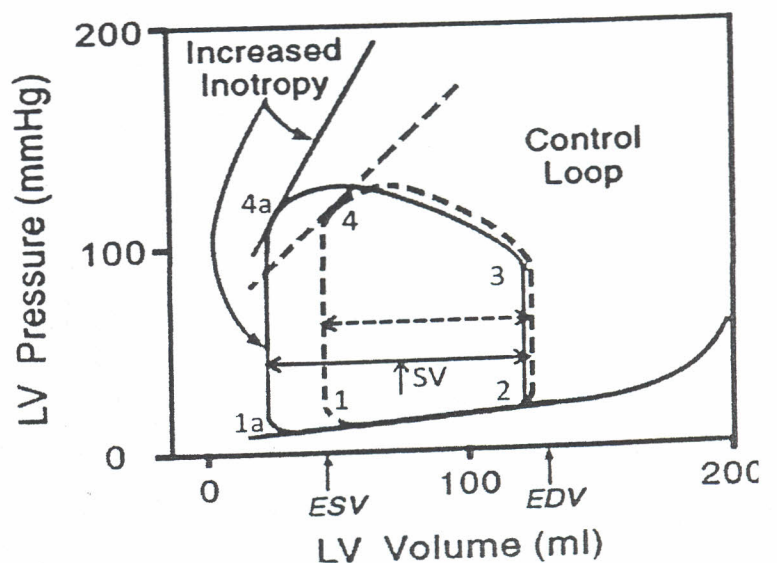


Figure (61): Effect of increasing inotropy on pressure-volume loop showing increased SV

- **+++ preload** → **+++ SV** (Frank-Starling's law) → **"heterometric autoregulatory mechanism"** (matches SV & CO with VR)
- **Using the ventricular pressure-volume loop:**
 - a. More ventricular filling (+++ preload) → higher EDV (2a)
 - b. Isometric contraction starts at (2a) till the same ventricular pressure (3) → aortic valve opens → Ejection starts till the end-systolic pressure (4) → aortic valve closes → Isometric relaxation occurs at same ESV (1)
 - c. +++ width of pressure-volume loop → +++ SV
 - d. +++ preload → +++ degree of shortening & +++ velocity of shortening → +++ SV
- **Several factors can affect ventricular preload:**
 1. +++ venous pressure & VR → +++ ventricular filling → +++ preload
 2. Strong atrial contraction → +++ preload.
 3. +++ HR (with constant VR) → ---- preload (no enough time for ventricular filling)
 4. ---- ventricular compliance (hypertrophy or myocardial infarction) → ---- preload

2- Effect of Afterload on Stroke Volume

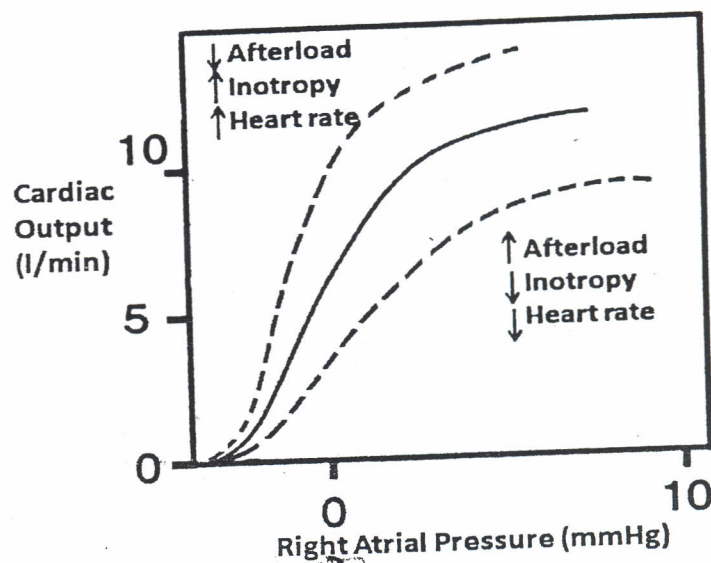
Afterload = load against which the ventricle contracts to eject blood = aortic pressure

- **At constant preload, +++ afterload** → ---- SV (shifts the preload & SV relationship downwards) (---- afterload has an opposite effect → shifts the curve upwards)
- **Using the ventricular pressure-volume loop:**
 - a. At Same EDV (2), the ventricle starts isometric contraction → +++ ventricular pressure to higher level (3a) (new higher afterload) → aortic valve opens
 - b. Ventricle ejection starts & ends at higher ESP (4a) & higher ESV (1a) → ----SV
 - c. +++ afterload → --- degree of shortening & --- velocity of shortening → ---- SV

3- Effect of Inotropic State on Stroke Volume

- **At constant preload & afterload, +++ inotropy** → +++ SV (shifts the preload & SV relationship upwards); ---- inotropy → shifts the curve downwards
- **Using the ventricular pressure-volume loop:**
 - a. Isometric contraction starts at same EDV (2) & ends at same afterload level (3)
 - b. Ejection continues till aortic valve closes (4a) on the shifted ESPVR line (up & left) by +++inotropy)
 - c. Ejection continues to a lower ESV (1a) → +++SV (+++ inotropy → ---- ESV)
 - d. +++ inotropic state → +++the degree & velocity of shortening → +++ SV

Figure (62): Cardiac function curve showing the effects of changing afterload, inotropy and heart rate.



Ejection fraction (EF)

- Fraction of the EDV that is ejected with each beat (normally >55% (or 0.55))
- EF is used clinically as index of contractility (+++ inotropy → +++ EF & vice versa)

$$\text{Ejection Fraction} = \frac{\text{Stroke Volume (SV)}}{\text{End Diastolic Volume (EDV)}}$$

Cardiac Function Curve

- It describes the relationship between right atrial pressure (RAP) & cardiac output (CO)
- It is an expression of Starling's law: +++ RAP → +++ CO;
- RAP represents the preload (pressure that fills the ventricle to its EDV)
- **Heterometric autoregulation** → Intrinsic mechanism → +++ CO independent of any external nervous or hormonal stimulation
- It is limited → heart pumps 13 L/min (2.5 times the normal VR) without nervous or hormonal stimulation. Further +++ in RAP → no further +++ in CO (plateau)

++++ slope of the cardiac function curve	----- slope of the cardiac function curve
<ul style="list-style-type: none"> ▪ +++ Heart rate (+++ sympathetic) ▪ +++ Inotropy (+++ sympathetic) ▪ --- Afterload (VD & --- ABP). <p>higher CO is achieved for same RAP; CO can exceed 13 L/min → "hyper-effective heart"</p>	<ul style="list-style-type: none"> ▪ ----- Heart rate (+++parasympathetic) ▪ ----- Inotropy (e.g. myocardial ischemia). ▪ +++++ Afterload (hypertension). <p>lower CO is achieved for same RAP; maximum CO decreases below 13 L/min → "hypo-effective heart"</p>

Cardiac Reserve CR

Maximum % +++ in CO achieved above normal in response to +++ body needs

- In normal young adult → CR = 300% - 400%; +++ CO from 5 L/min to 15-20 L/min (during maximal exercise)
- In well-trained athletes → +++ CR as high as 700% (35 l/min)
- In elderly people → ---- CR to 200% or even less
- In heart failure → ---- CR down to zero%

Cardiac reserve depends on the following mechanisms:

- 1- **Heart rate reserve**: maximal HR during maximal exercise can be estimated by this equation: Maximal heart rate = 220 – age in years
= 200 beats/min in normal young adults

Normal resting HR = 75 /min; it can +++ from 75 to 200/min during exercise (HR reserve)

2- **Stroke volume reserve**: SV = 70 ml in normal young adults; it can +++ up to 200 ml during maximal exercise by:

- a. +++ EDV (Frank-Starling's mechanism)
- b. ---- ESV (by sympathetic stimulation or other +ve inotropic stimuli)

3- **Increased size of the heart (cardiac hypertrophy)**:

- a. **Eccentric hypertrophy "volume overload hypertrophy"**: in well-trained athletes who perform endurance exercise (prolonged moderate intensity exercise: long distance runners) → +++ heart mass by 50-60% & +++ ventricular EDV → enables the heart to pump greater SV
- b. **Concentric hypertrophy "pressure overload hypertrophy"**: heart is exposed to prolonged high afterload (strength training) → +++ ventricular thickness with no +++ in ventricular volume → the ventricle can pump with greater strength without an +++ in wall stress. Then, ventricular compliance decreases (ventricle becomes stiffer) & ventricular filling may become deficient.